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A concise history of echocardiography: timeline, pioneers, and landmark publications

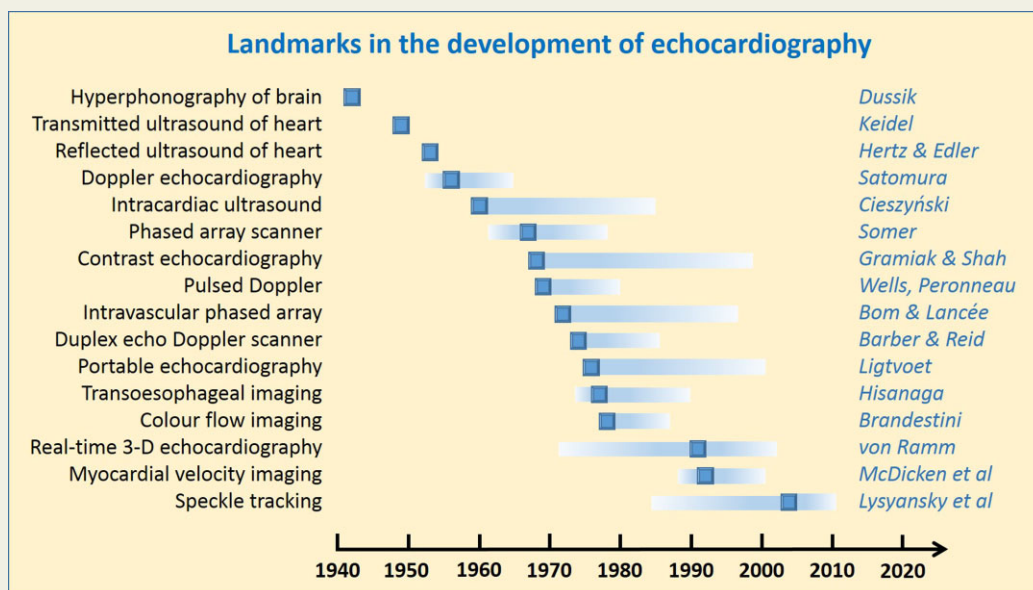
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Echocardiography is less than 70 years old, and many major advances have occurred within living memory, but already some pioneering contributions may be overlooked. In order to consider what circumstances have been common to the most successful innovations, we have studied and here provide a timeline and summary of the most important developments in transthoracic and transoesophageal ultrasound imaging and Doppler techniques, as well as in intravascular ultrasound and imaging in paediatric cardiology. The entries are linked to a comprehensive list of first publications and to a collection of first-hand historical accounts published by early investigators. Review of the original manuscripts highlights that it is difficult to establish unequivocal precedence for many new imaging methods, since engineers were often working independently but simultaneously on similar problems. Many individuals who are prominently linked with particular developments were not the first in their field. Developments in echocardiography have been highly dependent on technological advances, and most likely to be successful when engineers and clinicians were able to collaborate with open exchange between centres and disciplines. As with many other new medical technologies, initial responses were sceptical and introduction into clinical practice required persistence and substantial energy from the first adopters. Current developments involve advances in software as much as in equipment, and progress will depend on continuing collaborations between engineers and clinical scientists, for example to identify unmet needs and to investigate the clinical impact of particular imaging approaches.

Graphical Abstract



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Table 1 Cardiac and cardiovascular ultrasound timeline

Year	Scientific contribution
1727	James Bradley reported the aberration of light from stars, and measured its speed. ¹
1738	Daniel Bernoulli related the speed of a fluid to a local decrease in pressure or potential energy. ²
1757	Leonhard Euler (who had studied with Bernoulli's father) published general principles of fluid dynamics, ³ followed in 1775 by his publication on flow in blood that is still applicable to non-invasive haemodynamic assessments. ⁴
1842	Christian Doppler gave paper 'On the coloured light of the double stars and certain other heavenly bodies' ⁵ to the Royal Bohemian Society of Sciences, Prague, 25th May (which was a theoretical development of the earlier paper by James Bradley).
1845	Christophorus Hendrik Diederik Buijs Ballot, observed the frequency shift of sound waves. ⁶
1880	Jacques and Pierre Curie discovered the piezoelectric effect. ⁷
1916	Paul Langevin (who had been a doctoral student of Pierre Curie) developed SONAR during the First World War; he filed patents with Constantin Chilowsky in 1916 in France ⁸ and 1917 in the USA ⁹ (stating that 'The relative motion of the obstacle and the observation post may be determined by applying Doppler's method.').
1929	Sokolov in Russia proposed using ultrasound to test castings. ¹⁰ He filed a US patent application for his ultrasonic flaw detector (as Sergey Sokoloff) in 1937. ¹¹
1940	Floyd Firestone constructed an ultrasonic reflectoscope for industrial use. ¹² He applied for a patent during the Second World War, and published his method afterwards in 1946. ¹³
1942	Karl Theo Dussik developed what he called 'hyperphonography', using transmitted US to examine the brain, ^{14,15} he considered but did not pursue ultrasound reflection.
1949	Wolf-Dieter Keidel scanned the heart with transmitted ultrasound, to estimate its volume (after trying but rejecting the pulse-reflection method). ^{16,17}
1952	John Wild and John Reid applied echo-ranging to determine the structure of biological soft tissues (including breast). ¹⁸⁻²⁰ Figures include 'A-mode' demonstration. (John Wild started his research after locating to the USA in 1946).
1952	Douglass Howry & Roderic Bliss produced compound scans of human anatomy, equivalent cumulatively to 2D cross-sections ('Somascopes'), ^{21,22} first results obtained in 1950.
1953	May: first trial by Hellmuth Hertz and Inge Edler on themselves of ultrasound using machine from Kockum shipyard; first A-mode scan (reflected ultrasound) of heart.
1953	29th October, first M-mode scan by Edler and Hertz. Published 1954. ²³
1955	Ian Donald (who met John Wild in London in the early 1950 s) starts to investigate reflected ultrasound in the abdomen and then in obstetric practice, like Edler and Hertz starting with a borrowed flaw detector; with engineer Tom Brown, develops 'Diasonograph' which produced compound obstetric scans. ²⁴
1956	Shigeo Satomura, ultrasonic Doppler method to measure cardiac motion (with continuous wave). Initial report in Japanese, ²⁵ first publication in English in 1957. ²⁶
1960	Tomasz Cieszyński, first intravascular scanning and intracardiac echocardiography reported, using a single-element transducer on a catheter (developed from 1956). ²⁷
1961	Edler's thesis published as supplement to Acta Medica Scandinavica. ²⁸
1962	Ryozo Omoto obtained 2D intravascular images with a slowly rotating, single-element transducer mounted at a catheter tip. ^{29,30} First publication in English in 1967. ^{31,32}
1963	First dedicated cardiac ultrasound scanner built by John (Jack) Reid, working with cardiologist Claude Joyner. ³³
1963	Olofsson develops an optical mirror system for 2D scanning of the heart, ³⁴ working with Hertz. ³⁵ Further development reported by Arne Åsberg (1967). ³⁶
1964	'Ultrasono-cardio-tomography' reported from Sendai, Japan, for 2D imaging using mechanical sector scanning. ³⁷⁻³⁹
1967	Francis McLeod, directional Doppler system. ⁴⁰
1967	Jan Somer constructed first electronic phased-array scanner ('Electrosca'). ^{41,42}
1968	Raymond Gramiak and Pravin Shah, first report of (M-mode) contrast echocardiography. ⁴³
1968	Daniel Kalmanson, directional flow measurement by continuous wave Doppler. ⁴⁴
1969	Range-gated (pulsed) Doppler ultrasound developed by three groups: in 1969 Peter Wells ⁴⁵ (Bristol) and Paul Peronneau ⁴⁶ (Paris); and then Donald Baker ⁴⁷ (1970).
1969	Transthoracic (continuous wave) recording of aortic flow by Henry Light. ⁴⁸
1971	Nicolaas (Klaas) Bom and Charles Lancée, first real-time 2D (linear array) cardiac scans ('Multiscan'). ^{49,50}
1972	Bom and colleagues, first catheter-based cylindrical phased-array ultrasonic intravascular/intracardiac transducer. ⁵¹
1972	First textbook on echocardiography (Harvey Feigenbaum). ⁵²
1973	First clinical reports on 2D echo (using the Multiscan) by Frank Kloster ⁵³ and Jos Roelandt, ⁵⁴ with Bom and colleagues.

Continued

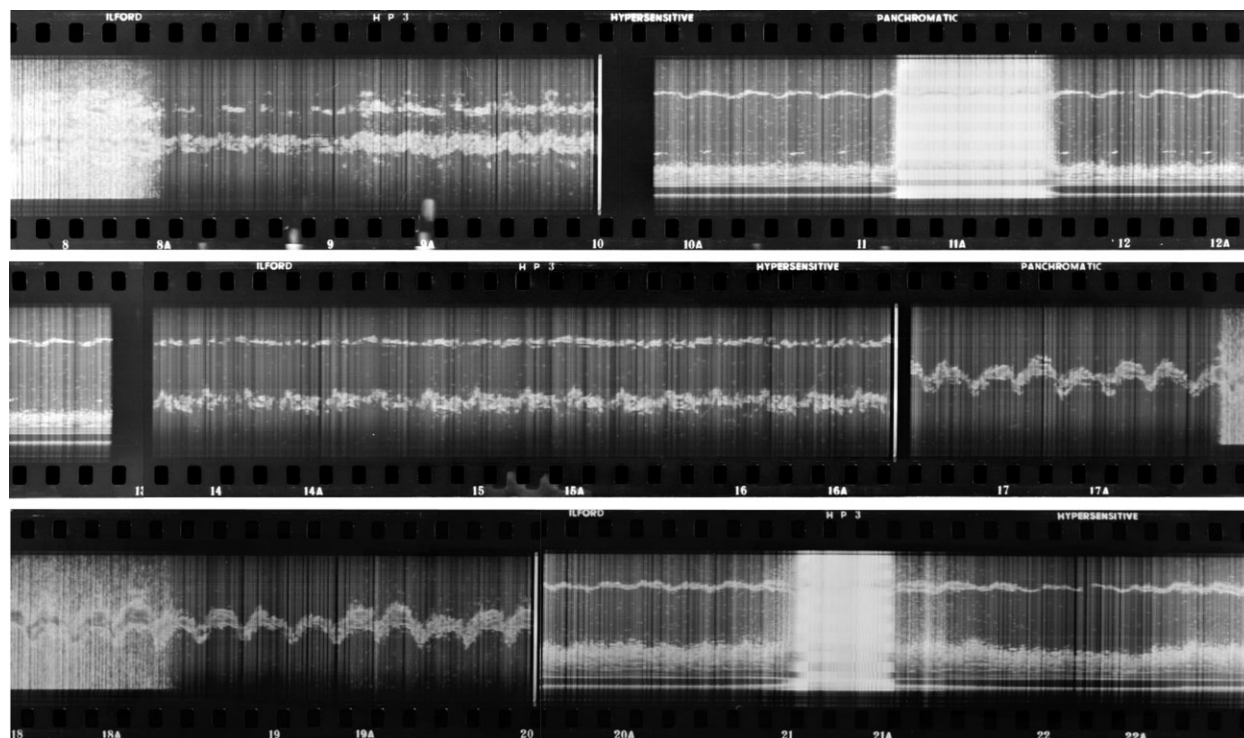


Figure 2 The first photographic film of M-mode echocardiography that was exposed by Edler and Hertz in October 1953, digitally scanned and then displayed as a continuous contact print. (courtesy of Professor Lars Edler)

Segal in 1966 and adopted by the American Institute of Ultrasound in Medicine.^{110,111}

Feigenbaum wrote the first textbook on 'Echocardiography', which was published in 1972.⁵² He and Richard Popp compared echocardiographic measurements with left ventricular volumes estimated by angiography.¹¹² Many other studies were performed in the early 1970s to validate M-mode measurements, including one by Popp that demonstrated the importance of using standard transducer positions.¹¹³

Two-dimensional echocardiography

Hertz had proposed cross-sectional or two-dimensional (2D) echocardiography before suitable technology was available, using a rotating mirror system (Figures 4A and 4B).^{34,114,115} Using this, in 1967 Åsberg reported that it produced sequences of 2D cardiac images which allowed cardiac motion to be followed.³⁶ In addition in the mid-1960s, investigators in Japan developed a prototype mechanical sector scanner that could produce a static 2D silhouette of the heart at any time during the heart cycle.^{37–39,116} That system was used by Teichholz *et al.* in 1974 to compare echocardiographic 2D images with biplane left ventriculography, to estimate volumes and validate their method of estimating ejection fraction from end-diastolic and end-systolic dimensions,⁶² while also recognizing its limitations.¹¹⁷

The first electronic phased-array scanner was constructed by Jan Somer in 1968,^{41,42} and other new transducers were developed in several centres during the early 1970s.¹¹⁸ A linear array was made at the Thoraxcentre in Rotterdam in 1971 by Nicolaas (Klaas) Bom and Charles Lancée^{49,50} and used in initial clinical studies by Jos Roelandt and Frank Kloster^{53,54} (Figure 4C). A mechanical sector

scanner was produced by Jim Griffith and Walter Henry,^{55,56} and a prototype phased-array scanner was built by Thurstone and Von Ramm and evaluated clinically by Joe Kisslo.^{57–59} Another mechanical sector scanner was developed around the same time, initially from a modified electric toothbrush, by Eggleton with Feigenbaum.^{120,108}

These scanners were employed in the early 1970s to identify regional wall motion abnormalities during spontaneous and induced myocardial ischaemia and after myocardial infarction.¹²¹ Inducible ischaemia was diagnosed using M-mode echocardiography by several investigators during the 1970s and then exercise stress echocardiography using cross-sectional imaging was reported first in 1979.⁷⁷ Others developed the technique using wider sector angles, in 1981.^{78,79} Pharmacological stress echocardiography using dipyridamole was proposed by Eugenio Picano and Alessandro Distanti in 1985¹²² and stress echocardiography using dobutamine by Luc Piérard and colleagues in 1986.¹²³

Three-dimensional echocardiography

The goal of three-dimensional (3D) imaging of the heart had been considered for a long time before progress in technology and computing could make it a realistic prospect. For example, in 1974 Dekker *et al.* registered the position of a probe attached to a mechanical arm, to reconstruct a 3D image after acquiring multiple 2D cross-sections.⁶¹ Others located the probe position and orientation with spark gap technology, or else they rotated the imaging plane mechanically from a stable probe position. All these original systems required external or internal reference systems to determine where the transducer was positioned in 3D space relative to the heart. Acquisition needed to be gated

can be fused in real-time with fluoroscopic images, to guide cardiac structural interventions by visualising catheters, contrast, tissue structures and blood flow, all spatially synchronized and superimposed.

Doppler ultrasound

There is a long history of the development of ultrasonic methods for recording and displaying blood flow and measuring its velocity in order to derive estimates of intracardiac pressure gradients. Although we apply the name of Christian Doppler, his original presentation in Prague in 1842⁵ was a theoretical development of an earlier study on the motion of distant stars by James Bradley,¹ without any new or original experimental observations.¹⁴⁰ A change in the frequency of sound waves as they are transmitted from a moving target or towards a travelling observer, was first demonstrated a few years later in the Netherlands by Christophorus Buijs Ballot who arranged for a train to travel past stationary musicians playing a constant note on a horn.⁶ He had been sceptical and was trying to disprove Doppler's hypothesis but in fact confirmed it.^{140,141}

Cardiovascular imaging applications now estimate velocities using autocorrelation to assess phase shift,¹⁴² rather than by calculating the Doppler shift in frequency or wavelength, but the eponymous attribution persists. Doppler echocardiography was developed during the 1950s in Japan by Shigeo Satomura, whose first investigations from 1952 were to measure heart motion rather than blood flow.^{25,27,143} In 1956 Yoshida with Satomura reported that Doppler ultrasound signals could be obtained from the human heart due to the motion of heart valves and blood flow.^{144,145} Other Japanese investigators correlated the observed phase shift with the velocity of the target, and related the amplitude of the signal to the number of red cells as reflectors.^{146,147}

In 1966 and independently, both Kato in Japan and Robert Rushmer in the USA reported that they had developed directional blood flow meters.^{148,149} A prototype apparatus for the continuous assessment of flow was also reported by Francis McLeod in 1967,⁴⁰ and another by Daniel Kalmanson in Paris in 1968 with the engineer Gérard Toutain.^{44,150} These machines recorded directional Doppler signals, meaning that it was possible to distinguish blood flow towards or away from the transducer, for example in the jugular vein of patients with right heart disease.¹⁵¹ About the same time, Light was using Doppler from a suprasternal approach to record aortic blood flow.⁴⁸ More significantly, range-gated or pulsed Doppler was being developed independently by three groups—Peter Wells in Bristol⁴⁵ and Paul Peronneau in Paris,⁴⁶ both reported in 1969, and Donald Baker in Seattle, published in 1970.⁴⁷ Thereafter the key advance was the development of a duplex scanner by Frank Barber in 1974, so that images and flow could be recorded using a single ultrasound system.⁶⁰ Griffith and Henry published details of another combined system in 1978.⁷⁴ Thus far, blood flow in the heart and vessels could be assessed only semi-quantitatively.¹⁵²

The first person to demonstrate (in 1976) that Doppler measurements of intracardiac flow velocities could be used to estimate pressure gradients was Jarle Holen, who had worked as an aerodynamics engineer at the Boeing factory in Seattle before studying medicine. He went from Rochester in New York state, where he had worked in the radiology department with Gramiak, to Oslo to undertake his

doctoral research. At first, the university department did not have an echocardiographic machine, and so a foetal monitor was modified to obtain Doppler signals. He then measured the velocity of flow across the mitral valve in patients with stenosis and calculated the gradients by an application of the Gorlin formula; the results correlated well with invasive measurements.⁶⁵ Some years later, in an *in vitro* experiment, he confirmed the accuracy of the new methods against pressures that were measured directly.¹⁵³

Independently, and from about 1974, Bjørn Angelsen at the Norwegian Technical University in Trondheim developed a combined pulsed and continuous wave Doppler system^{63,154} and proposed that gradients could be estimated using a simplification of the Bernoulli equation.⁷⁰ Liv Hatle was provided with a system built by Kjell Kristoffersen from Angelsen's group, and their first clinical study was presented by Brubakk at the European Congress of Cardiology in Amsterdam in 1976; it was met with some disbelief but Holen's paper came out shortly afterwards, confirming the results. Seminal publications followed from 1978 on the quantification of mitral stenosis,⁷⁵ aortic stenosis,⁷⁶ tricuspid regurgitation,¹⁵⁵ and right ventricular systolic pressure.¹⁵⁶ Investigators in Japan proposed that mitral and tricuspid flow velocities could be used to estimate left and right ventricular diastolic filling and function.^{85,157}

Colour flow mapping became possible after the development of a multigate pulsed Doppler system, first reported in the late 1970s by the engineer Marco Brandestini from Don Baker's group at the University of Washington in Seattle.^{71,72} His initial prototype superimposed colour flow on M-mode echocardiography, but it was soon followed by colour flow on a 2D display.⁷³ The first commercially available system was developed at the Aloka company in Japan, by the engineer Chihiro Kasai *et al.*, from 1982 and in collaboration with Ryozo Omoto who reported their initial clinical experience in 1984.^{83,84,158} In the same year, Rolf Jenni used a Diasonics multigate Doppler system to reveal varying flow patterns across the human aorta.¹⁵⁹

Myocardial velocity imaging

The proof of concept for recording a Doppler signal from the myocardium came from Isaaq in 1989,⁸⁶ after earlier attempts with related but different techniques by Yoshida¹⁴⁵ and Kostis.¹⁶⁰ The key advance was the development of a method by McDicken and Sutherland which adapted the colour Doppler algorithms for flow in a standard echocardiographic machine preferentially to display the high-amplitude, low-velocity signals from the myocardium.^{89,161} This was soon integrated into commercially available imaging systems by the Acuson company (as 'Doppler myocardial imaging') during the 1990s. A method was proposed for the post-processing of colour Doppler information to derive maps of other features of regional myocardial function,⁹⁰ and then methods were demonstrated for measuring local deformation of the myocardium as strain rate or strain.⁹¹ Doppler myocardial Imaging was introduced into paediatric cardiology from 2002.^{162,163}

Tracking the speckle pattern of ultrasound reflections, to obtain angle-independent images of blood flow and tissue motion, was suggested in 1991 but not feasible for implementation at that time because of insufficient computing capacity.¹⁶⁴ The first practical solution that became commercially available was developed by the General Electric company in Israel by the engineer Peter Lysyansky with clinical colleagues, in 2004.^{92,93} Although now widely applied,

the technique has insufficient temporal resolution to fully resolve regional myocardial strain rates.

Echocardiography in congenital heart disease

Following the introduction of low frequency (2.5 MHz) M-mode echocardiography into adult cardiology in the late 1960s, it was used at higher imaging frequencies (5.0 and 7.5 MHz) to study cardiac structure and function in children with congenital or acquired heart lesions. Whereas the anatomy of the cardiac chambers and vascular connections in most adults is predictable, the geometry of complex congenital malformations posed a great challenge for the M-mode technique. Despite this caveat, early diagnostic studies were reported in 1967¹⁶⁵ and 1971.¹⁶⁶ At that time the morphology of complex congenital cardiac lesions was poorly understood, but certain patterns on M-mode traces were described which could suggest underlying structural malformations such as transposition of the great arteries.¹⁶⁷ Nonetheless, the limitations of the M-mode technique for describing spatially complex lesions rapidly became evident.

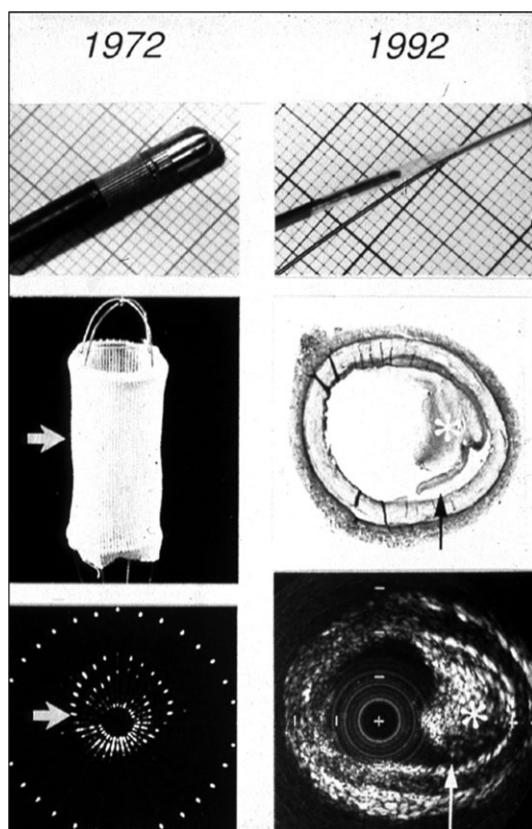


Figure 6 Left: 32-element phased-array 5.6 MHz intravascular ultrasound imaging (IVUS) of a basket (1972). Right: Single element rotating 30 MHz IVUS image of an artery containing atherosclerotic plaque (asterisk, and arrowed) (1992). From Bom N, Lancée CT, Rijsterborgh H, ten Hoff H, Roelandt JRTC. From idea to clinical application. *in* Intravascular Ultrasound, Roelandt, Gussenhoven, Bom Eds. Kluwer Academic Publishers, 1993.

Pioneering work on cardiac morphology by the Van Praeghs in the 1960s¹⁶⁸ and the Anderson group in the 1970s¹⁶⁹ was crucial for understanding and defining complex congenital cardiac malformations. By the early 1990s a series of studies had correlated echocardiographic findings with morphology, aided by the introduction of 5.0 and 7.5 MHz mechanical and phased-array 2-D imaging systems and by the development and integration of Doppler ultrasound modalities.^{170,171} Together, these led to the acceptance of cardiac ultrasound as a comprehensive and accurate modality to diagnose complex congenital heart disease.¹⁷²

Paediatric 2D sector scanning had been developed separately and in parallel with pulsed and continuous wave Doppler modalities, during the late 1970s. At first, the most successful systems were the mechanical rotational sector scanners developed by ATL, that imaged at 3.5 to 7.0 MHz. In parallel, Bjørn Angelsen and Kjell Kristoffersen^{63,154} developed their non-imaging pulsed and continuous wave Doppler system (which they called a pulsed-echo Doppler flowmeter, or PEDOF).^{63,154} It was tested clinically by Hatle and colleagues in Trondheim in 1976, and applied for the first non-invasive haemodynamic study of ventricular septal defects.¹⁷³ In 1982, the large Irex 111B duplex scanner was introduced, which for the first time combined 2D sector scanning with pulsed and continuous wave Doppler modalities.

Clinically effective colour flow mapping (CFM) was integrated into paediatric scanners by the mid 1980s, but again by two differing approaches. Vingmed (1986) and ATL based their CFM on rotational mechanical sector scanners, while Aloka (1987) introduced high-frequency phased-array scanners that imaged at 5.0 and 7.5 MHz. By the early 1990s, improvements in transducer ceramic materials allowed more crystals to be mounted, to produce an electronically steered matrix 2D array. Allied with new digital monitors and software-driven digital ultrasound machines, data could be acquired at high transducer frequency and displayed with high temporal and spatial resolution. These developments, combined with commercial considerations, led to the demise of mechanical sector scanners. Improvements in paediatric matrix probes, probe bus data transfer and machine processing speed, and digital displays, enabled real-time 3D transthoracic and transoesophageal echocardiography to be introduced to paediatric practice from the mid 2000s.^{174,175}

Foetal echocardiography

Ultrasound examination of the foetal heart was first described in 1966, using M-mode echocardiography,^{176,177} but it did not come of age until full integrated paediatric 2D ultrasound scanners became available from the late 1970s. Starting in 1980, Lindsey Allan produced a series of innovative reports on the intrauterine diagnosis of congenital heart disease, using both mechanical and phased-array sector scanners.¹⁷⁸ Once initial safety fears for the foetus had been addressed, this led to the widespread acceptance of trans-abdominal and trans-vaginal foetal echocardiography. New ultrasound modalities have been incorporated, including the assessment of intracardiac flows, myocardial deformation, and 3D imaging. Foetal echocardiography has become established as an essential discipline shared with obstetricians.

Intravascular ultrasound

In 1956, Tomasz Cieszyński built an ultrasonic catheter with the goal of applying it for intracardiac investigations, but his initial article reported experimental studies only (*in vitro* and in animals).²⁷ Dean Franklin's group at the University of Washington, Seattle, described an invasive ultrasound flowmeter in 1959, but it was clamped around the aorta rather than being intravascular and it was also assessed in animal experiments.¹⁷⁹ More studies were conducted by Ryoze Omoto *et al.*^{29–31,180} in Japan, while independently in Rotterdam in the early 1970s Bom *et al.*⁵¹ developed their first intravascular phased-array transducer, with 32 elements (Figure 6). Kalmanson recorded intracardiac signals from the right and left heart in 1979 and 1980, using directional Doppler.¹⁵²

After initial enthusiasm, interest in intravascular ultrasound (IVUS) was stalled until the mid 1980s when clinical impetus was provided by the development of percutaneous coronary interventions and by recognition that the X-ray shadow image of the lumen provided too limited information to develop balloon angioplasty, atherectomy, spark erosion, and other techniques safely. For that reason, IVUS was developed further.¹⁸¹ Bom *et al.* made a combined IVUS/spark erosion catheter and demonstrated its feasibility *in vitro* in 1988.¹⁸² Later, it was developed as a standalone IVUS system. In 1989 Paul Yock introduced a clinical rotating IVUS system, initially for imaging peripheral arteries and then for intracoronary imaging.¹⁸³ Its clinical application was confirmed for evaluating atherectomy and laser ablation.¹⁸⁴ Tobis *et al.* evaluated balloon angioplasty *in vitro*, using IVUS.¹⁸⁵ In addition in 1989, Hodgson introduced a clinical intracoronary phased-array imaging system, based on the 1972 patent from Bom and Lancée.¹⁸⁶

Backscatter analysis¹⁸⁷ and lessons learned from the analysis of images obtained *in vitro*¹⁸⁸ have played a major role in aiding the interpretation of IVUS images. Li *et al.*¹⁸⁹ developed semi-automatic lumen detection that was applied to assess the long-term effects of several stenting strategies and to compare the efficacy of statins. Several strategies for tissue identification have emerged, but none has yet been implemented into routine clinical practice. More recently, several 'sound and light combination' catheters have been developed, including an IVUS NIRS catheter (near-infrared spectroscopy) by InfraredX in collaboration with van der Steen and Serruys.¹⁹⁰

Conclusions

Although we have tried to locate and cite as many 'first' publications as possible, any retrospective exercise such as this is fraught with risks of inappropriate attributions or errors of omission. To minimize these, we have consulted the original publications and reviewed their reference lists, and when possible we have confirmed details with senior colleagues. We also reviewed historical accounts that have been published by principal investigators, which have been cited so that they can be consulted for more comprehensive details. Parallel developments in applications of ultrasound in other clinical fields have been reviewed recently by the European Federation of Societies of Ultrasound in Medicine and Biology,¹⁹¹ and other first-hand accounts of specific aspects of the history of echocardiography are available.^{192–194}

This endeavour has reinforced the view that it is often very difficult to establish scientific precedence. Clinical advances in echocardiographic imaging have been absolutely dependent on advances in technology, and when the intellectual climate was ripe and practical tools were available then many engineers and clinicians tackled similar challenges. There have been frequent occasions in the early history of ultrasound imaging when investigators were trying to solve the same problems but communication was less easy than now and publications were less accessible, and so they worked independently. As we have summarized, many individuals who are most prominently associated with particular developments have not been the first in their field. If that was part of the reasoning behind decisions not to award the Nobel prize for medicine to Edler and Hertz, then it may become apparent once the committee's deliberations are made available for review by historians after the usual 50-year embargo.

A second and obvious conclusion is that major advances have come from close collaborations between engineers and clinical scientists, so there is a need to ensure that such environments are developed and appropriately resourced. Although some researchers may be strongly motivated by competition, and careers can now be determined by metrics of academic productivity, in our opinion the most successful innovations have occurred when colleagues from different disciplines and different centres have been working together, preferably with an open and generous exchange of ideas. From an historical perspective what may be most interesting to current researchers is not what was done or by whom, but how the ideas and hypotheses were developed and where the original concepts came from—which is less often documented for posterity.

We have concentrated on describing the history of technological advances rather than clinical applications (*Graphical Abstract*), because that would have been an almost impossible undertaking. For practical reasons also, we have only briefly summarized the first steps in IVUS, which evolved from cardiac imaging but has now developed into an interventional subspecialty, and we have not reviewed vascular ultrasound or the development of hand-held systems. Echocardiography is still operator-dependent but that will lessen as machine learning methods are developed and implemented for acquiring, optimising, identifying and measuring images more accurately and reproducibly. Faster data transfer and processing would enhance the quality of 3D imaging and flow acquisition to such an extent that it could become standard practice, with all 2D, deformation and flow images and measurements being derived during post-processing, together with automated measurement of most parameters. While advances in software and artificial intelligence may transform clinical practice, it is too soon to include them in an historical overview. Similarly in our opinion the clinical utilities of recent technological developments such as high-frame-rate or ultrafast imaging, tissue characterisation by elastography, and the imaging of fluid dynamics, are still uncertain.

For the future, it could be particularly useful to establish some mechanism for expert clinical practitioners to reach a consensus on genuine unmet needs, since that has always been difficult and prone to individuals' expertise, interests and biases. As Henry Light wrote in 1992, what will be used may involve 'surrendering the ultimately desirable for the robustly measurable and eminently useful',¹⁹⁵ which implies a need for more epidemiological and outcomes-based evaluations. And hopefully, dialogue between clinicians and engineers

may overcome the problem identified by Hertz in 1973 that ‘.. different physicians had very different opinions on the relative importance of possible additional features and no clear answer could be given to the designing engineers in industry’.⁹⁶

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